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EXPLORING CHALLENGES AND SOLUTIONS IN HYDROGEL FAILURE AND FRACTURE MECHANICS FOR ADVANCING VASCULAR TISSUE ENGINEERING

Jeffrey Mawusi Drai¹, Aleksander Czekanski^{1*}

¹Mechanical Engineering, York University, Toronto, Canada

* alex.czekanski@lassonde.yorku.ca

Abstract—Vascular tissue engineering requires the creation of new materials that mimic the biomechanical and biofunctional properties of native tissues. Reinforced natural hydrogels are good candidates due to their biocompatibility, tunable mechanical properties, and support of cellular activities. Their application in vascular constructs is, nevertheless, hindered by inadequate information on their fracture and failure mechanisms under physiological conditions. This review introduces a comprehensive assessment of hydrogel fracture mechanics involving mechanical properties, toughness, and factors affecting failure like crosslinking density, porosity, and swelling stress. It provides a comparison among various theoretical tools, including linear and nonlinear fracture mechanics, theories of poroelasticity, and finite element analysis, as predictive tools for hydrogel. In addition to this, the review highlights how multiscale modeling plays a major role in transitioning from molecular-level interactions to macroscopic properties. Through the integration of theoretical models and empirical findings, this study reveals the shortcomings of existing methodologies and suggests directions for future research. The final objective of developing a better understanding of fracture and failure mechanisms is to enable the development of strong hydrogel-based materials for vascular tissue engineering.

Keywords: vascular tissue, fracture mechanics, tissue engineering, multiscale, reinforcement

I. INTRODUCTION

Vascular tissues are essential in the transport of nutrients, removal of metabolic waste, and control of blood pressure [1]. They are comprised of arteries, veins, and capillaries hierarchically structured to allow the exchange of nutrients and gases. The vascular system is also responsible for homeostasis and responds to injury by facilitating tissue repair at the site of injury. Aging, injury, and diseases can, however, destroy vascular tissues, resulting in such disorders as vascular occlusion, which may lead to ischemia and consequently, death.

One of the critical challenges in tissue engineering is to mimic functional vascularization, an essential feature of large-scale tissue constructs [2]. While breakthroughs have been reported

in tissue engineering of tissues including cartilage and skin, vascularized constructs for larger organs remain challenging to develop [1]. This indicates the need for establishing new materials and fabrication technologies in vascular tissue engineering.

Hydrogels, specifically Gelatin Methacryloyl (GelMA) and Alginate-based hydrogels, have been found to exhibit tunable mechanical behavior, biocompatibility, and the potential to support cell adhesion [3], [4]. GelMA hydrogels can be designed with regards to stiffness and degradation rates via methacrylation and are thus amenable to a wide variety of applications. Collagen-reinforced GelMA hydrogels have demonstrated the potential to be able to offer a scaffold for endothelial cell growth, a key aspect of vascularization [3]. However, their mechanical behavior, especially their resistance to fracture and failure under physiological loading, has been a concern.

This review theoretically investigates the fracture and failure mechanisms of natural hydrogels from the standpoint of fracture mechanics, materials science, and bioengineering. Through an investigation of gaps and limitations of current models, this study aims to suggest how hydrogel-based scaffolds can be optimized. The aim is to lay the groundwork for the development of more durable and longer-lasting vascular tissue engineering materials, thus enabling the creation of functional tissues.

II. FRACTURE AND FAILURE CHARACTERISTICS IN HYDREOGELS

A. Mechanical Behaviour and Fracture Mechanics

Hydrogels are materials that are renowned for their high-water content combined with a polymer matrix, which gives them excellent mechanical properties. The fracture mechanisms of these hydrogels are significantly different from those of conventional materials such as metals, polymers, and elastomers, because of which specialized investigation is needed to completely understand their behavior [5]. It has been demonstrated in earlier studies that the fracture toughness of hydrogels such as their resistance to crack growth, is controlled by a number of factors, including the structure of the polymer

network and the incorporation of reinforcing components like collagen [6]. It is important to understand the interaction between these factors in order to be able to predict the behavior of hydrogels under actual conditions of use, particularly for vascular tissue engineering.

B. Fracture Toughness and Measurement Techniques

Fracture toughness is a key parameter for measuring the resistance of hydrogels to crack propagation. The property is defined as the energy needed to propagate a crack in the material and, as such, is an essential factor in the design of hydrogels for load-bearing biomedical applications. Experimental methods to assess fracture toughness, along with theoretical models which elucidate these findings, have been under scrutinized examination within prior research [7]. Most specifically, a focus has been placed on the elongation criterion (Figure 1), through which it was demonstrated that the fracture behavior of hydrogels should be reconsidered based on network elongation [8]. This criterion recognizes the importance of deformation of hydrogel networks in fracture mechanisms, which gives a wider view of failure processes.

C. Factors Influencing Fracture and Failure

There are many factors that play a role in the fracture and failure behavior of hydrogels, each having a prominent influence on the mechanical stability of the hydrogel. A few of them include crosslinking density, the type of reinforcing material used, swelling behavior, porosity, and microstructural characteristics. Higher crosslinking densities, which is the concentration of crosslinking agents within the hydrogel, significantly improve the mechanical performance of hydrogels in terms of their stiffness and strength but at the cost of lowered flexibility [9] (Figure 2). Alternatively, the addition of reinforcement agents like collagen fibers within the hydrogel matrix assists in improving tensile strength and elasticity which enables a more ordered and stronger network to prevent localized failure and improve overall durability [10]. While swelling may be advantageous in some instances, excessive swelling threatens to produce structural damage and ultimately results in failure because of internal stresses. Indeed, research has determined that constrained swelling conditions result in fractures and thereby underscored the necessity of ascertaining the impact of swelling-induced stresses on material stability under physiological conditions [11]. Lastly, the existence of micropores within the structure of the hydrogel can significantly affect its fracture energy, which is a quantification of the material's capacity to dissipate energy as it fractures [12]. Computer simulations have shown that micropores improve intrinsic fracture energy through the facilitation of more uniform energy distribution in front of a crack tip [12]. This deliberate engineering of microstructure and porosity is therefore essential to move forward the mechanical properties of hydrogels.

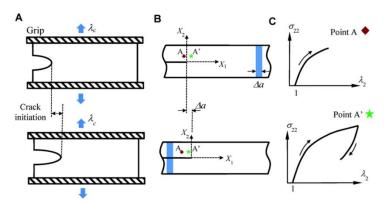


Figure 1: Fracture toughness of hydrogels - mechanism of measuring elongation criterion and interpretation [7]

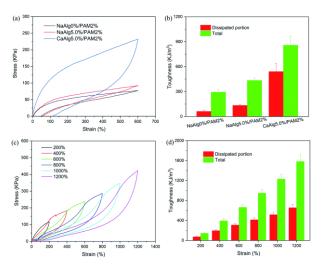


Figure 2:: Loading-unloading curves and the corresponding toughness of varying concentration of sodium alginate/poly(acrylamide) [13]

III. FRAMEWORKS FOR ANALYZING FRACTURE AND FAILURE IN HYDROGELS

A. Linear Elastic Fracture Mechanics (LEFM)

LEFM is a fundamental theory for analyzing crack initiation and growth in materials with linear elastic behavior. LEFM presents basic parameters like stress intensity factors and energy release rates that are important to predict fracture behavior. Nevertheless, hydrogels feature strong nonlinearity and large deformation, usually making the simplistic assumptions of LEFM hard to use [14]. As such, the immediate applicability of this model may be limited in the context of hydrogels, thus necessitating the investigation of more sophisticated frameworks that are able to capture their special material properties.

B. Nonlinear Fracture Mechanics (LEFM)

Due to the extreme deformability of hydrogels, nonlinear fracture mechanics offer an improved framework of study. They entail large strains and the intrinsic nonlinearity in the material response. For instance, the elongation-criterion approach offers a new perspective on the fracture behavior of hydrogels by emphasizing the importance of network elongation and its relation to microstructural changes [8] (Figure 1). By focusing on these aspects, one can achieve an understanding of the fracture toughness of the material that can inform the design of hydrogels with enhanced mechanical properties.

C. Poroelastic Model

The unique behavior of hydrogels to absorb water can lead to swelling, thereby creating internal stresses that may trigger fractures. Poroelastic models are responsible for the analysis of such occurrences because they excellently couple fluid flow and solid deformation [15]. With finite element simulations, researchers are capable of generating accurate simulations of stress distribution during swelling, which is fundamental in predicting occurrences of fracture. Knowledge of such interactions not only facilitates the evaluation of hydrogel stability but also provides information on the development of materials capable of resisting different environmental conditions.

D. Finite Element Method (FEM)

FEM is referred to as an effective computational method for modeling the intricate behaviors of hydrogels, such as fracture and failure mechanisms. This method facilitates the explicit definition of geometries of varied kinds and heterogeneous material properties, which makes it especially useful. Experiments run with the assistance of FEM have managed to model fracture in hydrogel, with detailed information on stress fields and failure conditions [16]. Through this technology, researchers can optimize the design of hydrogel, ultimately matching material behavior to the requirements of specific biomedical applications.

E. Phase-Field Models

Phase-field models offer a new continuum methodology to fracture mechanics research through the introduction of a continuous field to describe cracks, thus eliminating the necessity of following discrete crack trajectories [16]. The technique has been applied to simulate hydrogel fracture process, successfully capturing intricate crack patterns that are challenging to obtain using conventional techniques. Through a more intuitive understanding of failure mechanisms, phase-field models allow researchers to foresee the behavior of hydrogels under stress, thereby accelerating material development and application.

IV. DISCUSSION AND CRITICAL ANALYSIS

Synergy of Theoretical Frameworks and Experimental

Finite Element Modeling (FEM) is also crucial in the simulation of hydrogels' mechanical behavior. For instance, research has proven that the introduction of three-dimensionally printed poly(ε-caprolactone) (PCL) microarchitectures to GelMA hydrogels significantly improves their mechanical properties, something that is confirmed by FEM simulations [17].

Likewise, experimental research into the fracture characteristics of alginate gels has yielded data regarding their mechanical toughness (Figure 6), in addition to how parameters like the concentration of calcium ions influences the overall strength of the gel [18].

B. Challenges in Predicting Fracture and Failure

Precise fracture and failure prediction of new hydrogel biomaterials, e.g., GelMA-Alginate reinforced with collagen, is faced with a number of challenges, e.g., material heterogeneity, dynamic biological loading conditions, and scale bridging requirements. The composite character embedded within this hydrogel, and other such materials, brings about spatial mechanical property changes, thereby making predictive modeling even more difficult [19]. In vivo conditions involve many variables, including enzymatic breakdown and cell-cell interactions, that are challenging to simulate and forecast using theoretical models [20]. Moreover, merging data from molecular, microscopic, and macroscopic scales is a significant challenge [14], which has been persistently limiting the development of holistic models that can adequately explore the failure and fracture mechanics involved in hydrogels.

C. Importance of Multiscale Modeling Approaches

Multiscale modeling has also shown vast promise in filling the gap from molecular interactions to macroscopic mechanical properties. A multiscale mechanical model that incorporates multiple scales and spatial heterogeneity in the microstructure was able to accurately predict the failure of collagenous soft tissues and thus demonstrate the potential of such methods for hydrogel analysis [21]. Experiments show both adhesion and cohesion energies in hydrogels vary throughout the swelling process following specific scaling laws, which are related to the shear modulus, a critical parameter to know for the fracture behavior [22], [23] (Figure 3). By constructing multiscale simulation platforms, fracture mechanisms at early stages in hydrogel networks can now be explored and thus an investigation of network structures and their effects on mechanical properties can be made. This gives important insight for the development of hydrogels with improved fracture toughness.

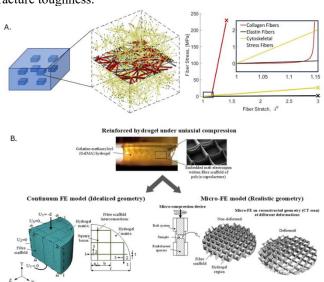


Figure 3: (A) Multiscale modeling connecting micro and macro properties of material for fracture analysis [24]. (B) Experimental corroboration of numerically estimated material parameters [25].

V. CONCLUSION

Understanding fracture and failure mechanisms in collagenreinforced GelMA-Alginate hydrogels is crucial in their application in vascular tissue engineering. Theoretical models need to be improved in future studies by incorporating the complex in vivo conditions like enzymatic degradation to better predict hydrogel performance. Additional consideration of the anisotropic properties imparted with collagen reinforcement will improve fracture outcome predictions. Multiscale modeling approaches are suggested to effectively consider these interactions. Also, establishing standard experimental protocols and using advanced imaging techniques, including real-time confocal microscopy and atomic force microscopy, will quantify the mechanical behavior of these hydrogels and map microstructural evolution with deformation and failure. These results will be essential to constrain theoretical models to best capture real material behavior.

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